

ORIGINAL ARTICLE

The importance of irradiance and area in neonatal phototherapy

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Background: Despite a long period of development, there are still considerable variations in the spectral output, the levels of irradiance, and irradiated area provided by commercial phototherapy systems. These variations depend on the types and output of the lamps used to produce the phototherapy, along with the design of the systems, and principally on whether the phototherapy is provided from overhead or underneath.

Objective: To see whether commercially available phototherapy systems produce sufficient irradiance over the surface area of the neonate.

Methods: Surface plots of the output irradiance were made on a number of systems and used to calculate the effective irradiance on the surface of a premature or term baby, using mapped outlines.

Results: A 10-fold difference in peak central irradiances was found between the systems tested, with a fourfold to fivefold difference in effective irradiance to the baby surfaces. Although work published over 20 years ago showed that levels of irradiance should reach 2 mW/cm² to achieve optimal effectiveness, some of the commercial systems tested do not appear to achieve this level.

Conclusion: Purchasers of neonatal phototherapy systems need to take into account whether the systems will produce sufficient irradiance over the area to ensure maximal effect, to keep the treatment time to a minimum.

A recent report from the American Academy of Pediatrics on neonatal hyperbilirubinaemia confirms the efficacy of phototherapy as a treatment.¹ Despite the long period of development since the original paper of Cremer *et al*,² there are still considerable variations in the spectral output, levels of irradiance, and irradiated area provided by commercial phototherapy systems. This was noted in the American Academy of Pediatrics report.

It is clear that the irradiance produced by phototherapy systems is an important factor. Many authors have shown that increasing irradiance produces a faster rate of fall of serum bilirubin.³⁻⁸ Tan⁹ showed over 20 years ago that irradiances of 2 mW/cm² (~40 μW/cm²/nm) are needed before a possible plateau response in the rate of bilirubin degradation is reached. Nevertheless, some current commercial phototherapy systems do not produce these irradiances.

Bringing the lights closer could increase the irradiance of overhead phototherapy systems. As this cannot easily be achieved for neonates in incubators, one solution is to provide phototherapy from underneath, as the neonate thus lies closer to the lights. This has been shown to be more effective than conventional overhead phototherapy.¹⁰ Another solution is to provide phototherapy from both above and below. This also seems to show a greater level of efficacy than overhead phototherapy alone.¹¹

The other parameter that affects the effectiveness of phototherapy is the area of the neonate irradiated by the system. Maisels⁸ highlighted the need to consider this issue, and it was also used by Dicken *et al*,¹² Vreman *et al*,¹⁴ and Wentworth¹⁴ in the assessment of the overall performance of phototherapy systems.

The above appear to confirm the idea that many conventional phototherapy systems do not produce sufficient irradiance to maximise the degradation of bilirubin.

If overhead phototherapy does indeed reach Tan's plateau value of optimum irradiance, logic suggests that the way to increase the effectiveness of phototherapy would be to

effectively double the treatment area by irradiating the neonate from below as well as above.

MATERIALS AND METHODS

The effective irradiance of a number of phototherapy systems was assessed by taking a series of irradiance measurements at 2 cm intervals in the illuminated field. Measurements were made using an International Light IL1700 radiometer with an SED033 detector, a "BR" bilirubin filter, and a "W" cosine diffuser. The radiometer and detector were calibrated against a secondary standard spectroradiometer, using a Philips TL52 phototherapy lamp as the light source.

All measurements for the overhead phototherapy systems were made with a source to measurement distance of 45 cm at the centre of the field, representing a typical treatment distance for neonates in incubators. For the fixed or underneath systems, measurements were made on the surface of the treatment area for that system, which included a blue-green gel mattress (JLJ Healthcare, Halesowen, West Midlands, UK). Measurements were made until the output had fallen to about 10% of the peak value or until the sides of the crib had been reached.

The method used for the irradiance mapping was similar to that used by Dicken *et al*¹² and Vreman *et al*.¹³ The data were entered into Excel spreadsheets and then linearly interpolated from the 2 cm grid used during the measurement process into a 1 cm grid to aid the mapping process. Outlines of both a premature and a term baby, similar to that of Vreman *et al*, were then mapped on to other spreadsheets. The only significant difference from the approach of Vreman *et al* is the use of an ellipsoidal model to simulate the curved edges of the body. This model suggested that the effective irradiance within 1 cm of the edge of the head and body should be reduced from 100% to 80%, and to 50% for the arms and legs, which reduces the overall effective irradiance by ~14%. Figure 1 shows the outline for the premature baby.

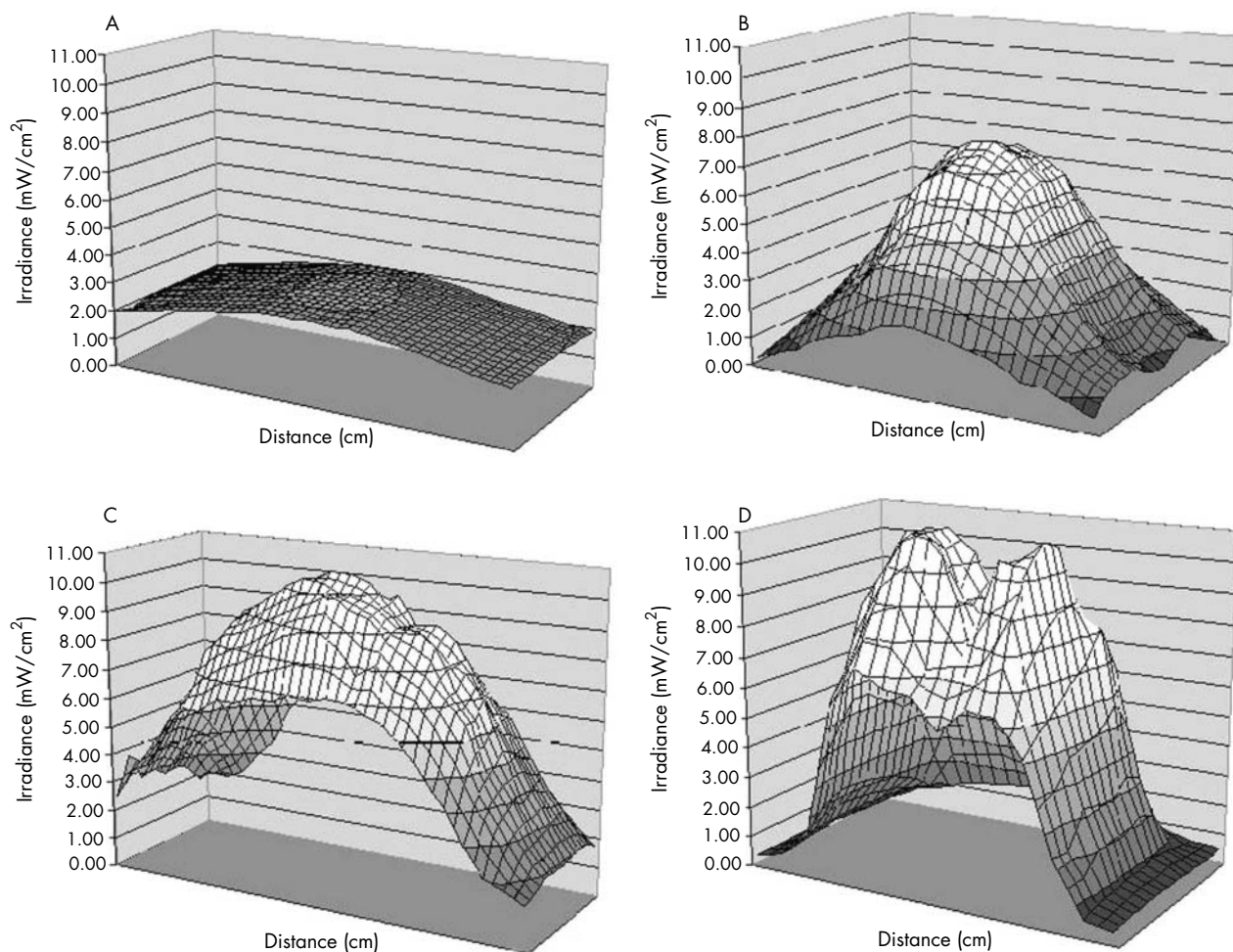


Figure 3 Surface plots for (A) IV2 (overhead), (B) Biliped, (C) IV2 (under), and (D) LED phototherapy systems. The plots show a three dimensional representation of the irradiance produced by the phototherapy systems over the area of the crib. Irradiance on the vertical axis is measured in mW/cm^2 . The horizontal axes represent distance on the crib surface.

- Medestime Bilicrystal IV2, a dual phototherapy system based on six blue compact fluorescent lamps in an underneath unit, with a further five compact fluorescent lamps in a fixed overhead unit;
- Medela Biliped, using a single blue compact fluorescent lamp underneath, with the baby lying on a blue-green gel mattress;
- A Medela Biliped, modified in-house at Bradford as an experimental unit. This unit contained $800 \times$ Nichia NSB500 blue LEDs as the light source, with the baby lying on a blue-green gel mattress.

Figures 2 and 3 show the surface plots of the different units tested. All surface plots are plotted on the same vertical scale to aid direct comparison of the systems.

Table 1 gives the results of the measurements and calculations of total surface irradiance for both term and premature neonates. The ratio figures were obtained by dividing the mean of the moved total irradiance figures by the central total irradiance.

DISCUSSION

The surface plots in figs 2 and 3 clearly show the large differences in measured irradiance of the systems tested. This is mirrored in the total irradiance figures given in table 1.

The plots appear to show that the systems with lower levels of irradiance have a more even irradiance field than the

higher output systems. Although this is true in absolute terms, the lower irradiance systems also show a similar percentage fall between centre and edge.

Three of the systems tested did not reach Tan's $2 \text{ mW}/\text{cm}^2$ central irradiance figure and also delivered lower total effective irradiances, which implies that they will not be as clinically effective as units that produce a greater level of irradiance.

Bringing the overhead units closer to the surface of the neonate would undoubtedly increase the measured irradiance, as the irradiance from an extended source is approximately proportional to $1/\text{distance}$ from the source. This is usually not an option for a neonate being treated in an incubator, and for neonates in cribs the level of heat generated by the lights also has to be taken into account.

The underneath systems show a significantly higher level of irradiance than the overhead systems, principally because of the closeness of the light sources to the baby's skin surface. In these systems, the light has in fact been attenuated by the use of the gel mattress, which scatters the light and reduces the irradiance at the surface of the neonate by about 30%. Use of a less attenuating surface would lead to a further increase in the irradiance.

The surface plot for the experimental LED array (fig 3D) shows a bimodal irradiance distribution, caused by the layout of the LEDs in two square panels with a small central gap. The resolution of the reduced irradiance between the panels

Table 1 Peak and integrated irradiances of the systems under test, together with the ratios of the total irradiance when the outlines were moved 4 cm and 8 cm

	Central peak irradiance (mW/cm ²)	Central peak irradiance (μW/cm ² /nm)	Term baby total irradiance at centre (mW)	Prem baby total irradiance at centre (mW)	Ratio 4 cm:centre	Ratio 8 cm:centre
Hill-Rom Microlite	1.20	~24	319	236	0.98	
Draeger Phototherapie	1.70	~34	575	366	0.97	0.97
Medestime Duo	1.72	~34	628	394	0.99	0.97
Natus neoBLUE	3.26	~65	1118	711	0.97	0.95
Bilicrystal IV2 (top unit)	3.08	~62	1034	684	0.99	
Bilicrystal IV2 (under unit)	10.57	~211	2744	2033	0.97	
Medela Bilibed	7.82	~156	1156	953		
LED Bilibed	11.72	~234	1333	1215		

shows the sensitivity of the method to changes in the shape of the light field.

Although there is a clear relation between the central irradiance value and the overall total irradiance figures for the term and premature baby outlines, they do not correlate perfectly. This is because of differences in the shapes of the light fields, and shows that both the peak irradiance and the area irradiated must be considered when seeking to assess the overall likely clinical effectiveness of the system.

Moving the outline by either 4 cm or 8 cm over the irradiated field did not appear to lead to a significant change in the level of irradiance. This was not done for either the Medela Bilibed or the modified unit containing the LED array, as the units are designed so the baby remains in a fixed position relative to the lights.

The irradiance measurements here were all made with a fixed bandwidth broad band radiometer. Maisels⁸ reminds us that we have to be careful about “measuring” irradiance, and Costarino *et al*¹⁵ go further, saying that “information obtained from a fixed band width radiometer designed to measure radiant flux in the blue light range may not allow meaningful comparison of phototherapy units in the clinical setting”. This problem occurs because of the widely differing spectra of phototherapy systems. Some authors have decided to use spectroradiometric measurements, such as Wentworth,¹⁴ who integrated the spectra from 400–550 nm.

However, using this kind of technique means that wavelengths outside the usually accepted action spectrum will contribute to the “useful” measured irradiance. The BR filter attached to the detector in our measurements is set to allow wavelengths in a 50 nm band centred on 450 nm, to match the action spectrum of Cremer *et al*.² The comments of Costarino *et al*¹⁵ assume that wavelengths outside the blue region make a positive contribution to phototherapy. If this is not the case, however, measurement devices such as the one used here do indeed provide a reasonable way of assessing the useful irradiance of phototherapy systems. Most evidence thus far appears to support the action spectrum of Cremer *et al* and so this was used.

Reviews such as those produced by the UK’s Medicines and Healthcare Products Regulatory Agency highlight the value of comparing systems using the same measurement techniques and equipment.¹⁶ This paper also shows that direct comparisons can show significant differences between commercially available systems of both the central and total effective irradiance over the surface of the neonate.

Purchasers of neonatal phototherapy systems need to take into account whether the systems will produce sufficient irradiance over the area required to ensure that the phototherapy is maximally effective, as this is likely to reduce the time that the neonate needs to undergo the treatment.

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